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Exhibit B

**Copy of the substitute specification with markings showing all changes
relative to the priority application**

Device For Connecting A Longitudinal Carrier To A Bone Fixation Means

BACKGROUND OF THE INVENTION

[001] The invention relates to a device for connecting a longitudinal carrier, for example, a longitudinal spinal rod, to a bone fixation means, for example, particularly a pedicle screw according to the generic term of Patent Claim 1.

[002] Certain devices Devices are already known in from the state of the art for connecting pedicle screws to longitudinal carriers for fixing the vertebral column. For example, United States Patent No. Such a connection device is disclosed in the US patent US 5,584,834 to Errico ERRICO This well known invention comprises discloses a device that allows a pedicle screw, or more generally for connecting a bone fixation anchoring element to be connected in a simple way to a longitudinal carrier.

[003] The connection device generally consists of a cylindrical central body, which is provided at its lower end with a slotted, externally conical collet chuck with tapered outer surface and a hollow-spherical cavity for receiving a spherical head of a bone fixation anchoring element and has an externally threaded at its upper end. In its central section, this the central body includes is provided with a channel hole, opened on the side, and running perpendicular to the its central axis for receiving the a longitudinal carrier. The connection device further includes a locking collar and a rod securing sleeve. The locking collar has an inner tapered surface A lower shell with an inner cone corresponding to the outer tapered surface formed on the lower end cone of the central body while the rod securing sleeve has and an upper shell with a passage opening towards the locking collar lower shell are pushed over this central body. When in the assembled state, both shells can be pressed downward the locking collar and the rod securing sleeve are axially displaceable with respect to the central body by means of a nut, which can be screwed over the external thread formed on the upper end of on the central body. In use, the The longitudinal carrier is inserted between the lower and upper shell, which is conducted through the locking collar and the rod securing sleeve so that the longitudinal carrier passes through the channel passage opening in the upper shell on the side formed in the central body and the passage formed in the rod securing sleeve. When the connection device is blocked, the upper shell is pressed downwards when this nut is tightened, Thereafter, rotation of the nut causes the rod securing sleeve to move downwards, which presses the longitudinal carrier inserted in the passage opening channel onto the lower shell, the inner cone of which as a result is shoved over the external cone of the collet chuck. When the cones are thus pressed onto each other it leads to

~~the collet chuck being compressed and thus the spherical head tensioned within the collet chuck being blocked. locking collar, which, in turn, causes the inner tapered surface of the locking collar to pass over the external tapered surface of the central body. As a result, the lower end of the central body compresses, which causes the position of the spherical head of the bone fixation element which is received within the hollow-spherical cavity of the central body to be fixed.~~

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[004] The disadvantage of this prior art device is, on the one hand, the significant construction height of the connection element due to the connection in the form of a socket joint between the ~~in part to the ball and socket type connection between the spherical head of the bone fixation anchoring element and the central body collet chuck~~ and, on the other hand, the space required for the surgical instrument for tightening the nut ~~to be screwed~~ over the external thread formed on the upper end of ~~on~~ the central body.

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SUMMARY OF THE INVENTION

[005] The invention is intended to remedy this situation. The invention ~~is based on the task of creating~~ discloses a device that requires as little space as possible and ~~which~~ can 15 additionally be implanted with a ~~minimum requirement for reduced number of surgical instruments and steps operations. Specifically, it would be preferable, It should specifically be possible to insert the implant with~~ a surgical instrument ~~which has~~ with a diameter ~~no~~ not larger than the diameter of the implant so that as little damage as possible is caused to the surrounding tissue parts.

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[006] The invention ~~solves the set task with~~ discloses a device for connecting a longitudinal carrier to a bone fixation means, specifically a pedicle screw, ~~which has the features of Claim 1. the device includes a connection element having a central axis, an external surface, an upper end, a lower end, a cavity extending coaxially along the central axis from the upper end to the lower end, the cavity having a reduced diameter portion at the lower end thereof, thereby forming at least one shoulder therein. The connection element further including a transverse channel passing through the connection element for receiving the longitudinal carrier. The device also includes a sealing cap having a front end, a rear end, a second cavity opening at the front end for receiving the connection element, and a second channel extending transversely to the central axis opening towards the front end for receiving the longitudinal carrier inserted within the transverse channel. The sealing cap may also incorporate tensioning means for fixedly securing the position of the longitudinal carrier. The device is characterized in that the connection element and the sealing cap contain complementary arresting means for securing the sealing cap to the connection element.~~

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[007] In a further embodiment of the ~~The~~ device according to the invention, ~~the device~~ essentially comprises a connection element with a sealing cap and a tensioning means. The connection element ~~has a~~ is provided with a cavity coaxial to the central axis, ~~an upper end, a lower end, and a cavity extending coaxially along the central axis from which is open at the upper end to and at the lower end of the connection element.~~ The cavity has a reduced diameter section at the ~~is tapered towards its~~ lower end of the connection element which forms by means of a shoulder. ~~The connection element further includes a transverse~~ A channel that is open at the upper end of the connection element so that a longitudinal carrier and running transverse to the central axis of the connection element penetrates the connection element diametrically, with the result that, for example, a longitudinal carrier representing a vertebral fixation system can be received within the channel, substantially and runs orthogonal to the central axis, whereas a bone fixation means, for example, a pedicle screw can be introduced conducted through the cavity parallel to the central axis, until the screw head of the pedicle screw rests on ~~is arrested axially~~ by the shoulder formed in the cavity. The sealing cap is provided with a second channel, which is also arranged transverse to the central axis and which is opened towards the front end of the sealing cap so that, wherein the longitudinal carrier may be is received by at the sealing cap when the sealing cap is installed on the connection element. ~~The~~ This second channel divides means that the sealing cap is divided from its front end to the base of the second channel in into two segments, which are elastically deformable with respect transverse to the central axis so that, in use, the sealing cap may be fixed with respect to the connection element by arresting means. The tensioning means can be connected to this at the rear end of the sealing cap may further include tensioning means, which, when tightened, fix the position of the and serves to block a longitudinal carrier and the a bone fixation means with respect to in the connection element. For securing the sealing cap to the connection element arresting means latching into each other are arranged complementary to each other on the connection element and in the cavity of the sealing cap.

[008] In the preferred embodiment of the device according to the invention, the arresting means are arranged on the periphery of the connection element and also on at the periphery of in the cavity in the sealing cap. The arresting means preferably includes a plurality consists of bulges formed on the connection element and a plurality of the complementary depressions formed in the cavity of the sealing cap.

[009] In another embodiment of the device according to the invention, the shoulder that narrows the cavity at the lower front end of the sealing cap comprises a planar bearing surface for receiving and supporting This bearing surface is used as a support, for example, for the screw

head of a pedicle screw. Alternatively, the ~~Instead of the planar design, this~~ bearing surface can also be designed in spherical form or having several concentric steps.

[0010] ~~Further advantageous embodiments of the invention are indicated in the dependant claims.~~

5 [0011] ~~The advantages achieved by the invention can be seen essentially in that due to the device according to the invention: The present invention provides a device with a very low structural height. of the connection element with sealing cap can be achieved; Moreover, the present invention provides a the device which can maintain the longitudinal carrier within the transverse channel formed in the connection element be blocked during the implant operation by means of a single locking mechanism.; and The present invention also provides a device which can facilitate installation by way of an instrument which has instruments can be used that have a diameter less than the diameter of the implant, thus minimizing the size of the incision needed for accessing the operational site, which, in turn, reduces the amount of patient trauma and making which means there is now no need for any large access that can traumatisise the patient~~

10 ~~and the device is accordingly ideal for minimum invasive or navigated surgery. These implants also offer a possibility of treating patients in cases of thorascopic access.~~

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[0012] ~~In a further embodiment the device according to the invention may include comprises securing means which narrows by means of which the cavity formed in the connection element is narrowed between the rear end of the bone head of the bone fixation means and the upper end of the connection element so that. This prevents the bone fixation means can not pass through in the connection element from falling out at the upper end of the connection element. This enables the implants to be This embodiment design with securing means provides the advantage that pre-assembled thus reducing the amount implants are used which means less of time needed in the operating room and also reducing the risk in the operation theatre can be avoided and the risk potential, for example, of through mixing up or incorrectly inserting the bone fixation means into the connection elements. insertion is significantly reduced.~~

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[0013] The invention and further developments of the invention are described in more detail below on the basis of partially schematic illustrations of several embodiments.

BRIEF DESCRIPTION OF THE DRAWINGS

30 [0014] Fig. 1 shows a longitudinal section through the preferred embodiment of the device according to the invention;

[0015] Fig. 2a shows a view of the connection element of the embodiment of the device according to the invention illustrated in Fig. 1;

[0016] Fig. 2b shows a view of the embodiment of the device according to the invention illustrated in Fig. 1;

[0017] Fig. 3 shows a longitudinal section through another embodiment of the device according to the invention;

5 [0018] Fig. 4 shows a view of the embodiment of the device according to the invention illustrated in Fig. 3;

[0019] Fig. 5 shows a longitudinal section through a further embodiment of the device according to the invention; and

[0020] Fig. 6 shows a longitudinal section through a further embodiment of the device 10 according to the invention.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0021] Fig. 1 illustrates a bone fixation means 1 designed as a pedicle screw together with a connection element 5, a longitudinal carrier 11, a sealing cap 12 axially displaceable ~~shoved coaxially over the upper end 6 of the connection element 5 from its upper end 6 and a~~

15 ~~tensioning means 13, i.e., a set screw, incorporated into connected to the sealing cap 12. The bone fixation means 1 includes a front segment 3 and a rear segment 4, as shown, the~~ The front segment 3 of the bone fixation means 1 is designed as ~~has~~ a screw shaft 24 with external thread 26 so that the bone fixation means 1 may threadedly engage a patient's pedicle, while, whereas the rear segment 4 ~~has is designed as~~ a circular-cylindrical screw head 30 ~~having~~ . The bone

20 ~~fixation means 1 designed as pedicle screw can be screwed into a pedicle by means of the external thread 26 on the screw shaft 24, wherein a screwdriver (not illustrated) can be inserted in the~~ means 29, illustrated as a hexagon socket, for receiving a screwdriver, which are arranged at an end ~~position~~ on the screw head 30. Alternatively, the means 29 for receiving a screwdriver may be in the form Instead of a design as hexagon socket, the means 29 for receiving a screwdriver can also be designed as, for example, hexagon socket, Torx or Phillips.

25 [0022] As shown, the The connection element 5 generally is in the form consists of a hollow body having a coaxial to the central axis 2, with an upper end 6, and a lower end 7, and a cavity 8. The diameter of the cavity 8 formed in the connection element 5 is configured so as to have a reduced diameter portion tapered at the lower end 7 of the connection element 5, thus

30 forming, which forms a shoulder 9 with a bearing surface 25, preferably a planar bearing surface, on which the screw head 30 of the bone fixation means 1 can be placed. The lower end 7 of the connection element 5 is further configured so that the The screw shaft 24 of the bone fixation

means 1 can be passed through the reduced diameter portion eavity 8 tapered at the lower end 7 of the connection element 5. The connection element 5 further includes is furthermore penetrated vertically to the central axis 2 by a first channel 10, generally extending transverse to the central axis 2, wherein the this first channel 10 is open towards the upper end 6 of the

5 connection element 5 so that the longitudinal carrier 11 may be inserted into the first channel 10 from the top. The depth of the channel 10 being sized and configured to receive the longitudinal carrier 11. More specifically, the The depth of the channel 10, measured from the upper end 6 of the connection element 5 parallel to the central axis 2, is designed in such a way that a longitudinal carrier 11 is inserted into the channel 10 above can be placed at an end position on 10 the screw head 30 of the bone fixation means 1.

[0023] The sealing cap 12 is sized and configured so that, in use, the sealing cap 12 is axially displaceable, i.e., pushed, over the connection element 5 so that wherein the front end 20 of the sealing cap 12 is directed towards the lower end 7 of the connection element 5 and the connection element 5 is partially received parallel to the central axis 2 in a the second cavity 18 15 formed provided in the sealing cap 12. The sealing cap 12 also incorporates a second channel 17 penetrating the sealing cap 12 vertical to the central axis 2 which enables the acceptance of the longitudinal carrier 11 inserted laid in the connection element 5 in the first channel 10 to be received in the sealing cap 12. The second channel 17 is open at the front end 20 of the sealing cap 12 so that, in use, when with the result that the sealing cap 12 is axially displaced over the 20 connection element 5, the second channel 17 receives the in the case of longitudinal carrier 11 inserted in the connection element 5 can be pushed over the connection element 5 parallel to the central axis 2.

[0024] The device may also include When viewed parallel to the central axis 2, the arresting means 21 for securing the connection element 5 and the sealing cap 12. More 25 specifically, the outer surface of the connection element 5 may include bulges 15 while the inner surface of the sealing cap 12, and more specifically, the inner surface of the second cavity 18, includes complementary depressions 16 for engaging the bulges 15. Preferably, the connection element 5 and the sealing cap 12 include a plurality of arresting means 21 so that different latch positions are possible. That is, preferably, the arresting means 21 includes a plurality of bulges 30 15 and a plurality of depressions 16 so that when the first depression 16 has been pushed over the first bulge, i.e., the first latch position, the longitudinal carrier 11 may still be longitudinally moved with respect to the bone fixation means 1 so that the bones and/or bone fragments affixed thereto may be repositioned. However, as the sealing cap 12 is further axially displaced over the connection element 5 such that subsequent bulges 15 are aligned with subsequent depressions

16, the longitudinal carrier 11 becomes fixed with respect to the bone fixation means 1, are designed as bulges 15 attached peripheral to the connection element 5 and complementary depressions 16 attached peripheral in the second cavity 18 of the sealing cap 12. The arresting means 21 are arranged in the same design on two axial levels which means that different latch positions are possible. The first latch position is used preferably for repositioning the bones or bone fragments to be fixed, whereas the second or further latch positions are used for fixation of the device.

[0025] Preferably, as shown, the The bulges 15 and the depressions 16 are provided with a saw-tooth shaped profile, when viewed in a cross section surface parallel to the central axis 2, so that wherein the steep flanks of the bulges 15 are oriented towards the lower end 7 of the connection element 5 and the steep flanks of the depressions 16 are oriented towards the rear end 19 of the sealing cap 12 such that, in use, as If the sealing cap 12 is axially displaced shoved over the connection element 5 parallel to the central axis 2, the sealing cap 12, and more specifically, the two segments 27, 28 (Fig. 2b) of the sealing cap 12 formed by the second channel 17 are more easily biased apart, i.e., resiliently spread transverse to the central axis 2. This enables with the result that the sealing cap 12 to pass can be shoved over the bulges 15 formed on the connection element 5 until the bulges 15 align with the depressions 16 formed in the second cavity 18, at which point cover the bulges 15 and the two segments 27, 28 (Fig. 2b) on the sealing cap 12 elastically lock towards the central axis 2 resiliently move back, i.e., elastically move towards the central axis 2, so that the bulges 15 engage the depressions 16.

[0026] The sealing cap 12 may further incorporate The tensioning means 13, which as shown is are provided in the form of a set locking screw that can be screwed into an the internally threaded in the hole 31 formed at the rear end 19 of the sealing cap 12 coaxial to the central axis 2. Rotation of the tensioning means 13 causes the tensioning means 13 to press against the longitudinal carrier 11, which in turn causes the longitudinal carrier 11 to press against the head 30 of the bone fixation means 1 resulting in the head 30 being clamped between the shoulder 9 formed at the lower end 7 of the connection element 5 and the longitudinal carrier 11 thereby fixing the position of the bone fixation means 1 together with the longitudinal carrier 11 with respect to the connection element 5.

[0027] Fig. 2 shows the connection element 5 from the perspective of the upper end 6. As shown, the The cavity 8 and the arresting means 21 are arranged concentrically about to the central axis 2 (Fig. 1), wherein the arresting means 21 is configured in the form of bulges 15 that are, when seen parallel to the central axis 2, arranged on the outer circumference of peripheral on the connection means 5. The ring-shaped side wall of the connection element 5 and the bulges 15

are interrupted by the channel 10, wherein the channel axis 14 runs transverse vertical to the central axis 2 (Fig. 1).

[0028] The longitudinal carrier 11 is inserted in the channel 10. In addition, the channel 10 forms, on the connection element 5, forms two sidewalls tongues 22, 23 for on a section of its length, wherein the bulges 15 are provided only on at these two sidewalls tongues 22, 23 and do not surround the entire connection element 5.

[0029] Fig. 2b shows the sealing cap 12 with the tensioning means 13 assembled onto with the connection element 5 and the tensioning means 13. As shown, the The second channel 17 formed in penetrates the sealing cap 12 forms on one section of its length vertical to the central axis 2 (Fig. 1), with the result that two segments 27, 28 in are formed on the sealing cap 12, which resiliently spread radially when the sealing cap 12 is axially displaced, i.e., pushed, over the connection element 5, which allows the sealing cap 12 to be pushed over the bulges 15 formed on the connection element 5 (Fig. 1). As soon as the sealing cap 12 is displaced pushed far enough over the connection element 5 so that the depressions 16 (Fig. 1) in the sealing cap 12 align are able to engage with the bulges 15 formed on the connection element 5 (Fig. 1), the two segments 27, 28 will narrow elastically snap back, i.e. towards the central axis 2 (Fig. 1), wherein the bulges 15 formed on the connection element 5 will engage the depressions 16 formed on the sealing cap 12.

[0030] The embodiment of the device according to the invention illustrated in Fig. 3 and Fig. 4 differs from the embodiment illustrated in Figs. 1 and 2 only in that the sealing cap 12 is provided with two slots 34 orthogonal to the second channel 17, which are formed in inserted into the wall of the sealing cap 12, the slots 34 extending from the its front end 20 of the sealing cap 12. The slots 34 divide Instead of the two segments 27, 28 (Fig. 2b), the sealing cap 12 into in this embodiment is provided with four segments 27, 28, 32, 33 thereby increasing This means that the elasticity of the sealing cap 12 so that the sealing cap 12 may be more easily axially displaced can be increased and this cap can be shoved more easily over the bulges 15 formed on the connection element 5 as compared to a sealing cap 12 having only two segments 27, 28 as described above.

[0031] In use, For implanting the device, the pre-assembled implant comprising the bone fixation means 1 and the connection element 5 may be is removed from an the implant carrying container by with a screw driver which engages inserted in the means 29, without any need for a further instrument for holding the implant parts and without a the surgeon having to the join the bone fixation means 1 and the connection element 5 parts together. Thereafter, the pre- assembled implant may be Then, the implant which provisionally consists only of bone fixation

means 1 and a connection element 5 is screwed into the prepared pedicle. After the longitudinal carrier 11 is inserted ~~laid~~ into the first channel 10 arranged in the connection element 5, the same screwdriver may again be ~~is~~ used to remove again the pre-assembled sealing cap 12 provided with the tensioning means 13 from the implant carrying container, in which operation there is

5 again no need for a special holding instrument. By means of a special clamp, the sealing cap 12 is locked into the first latch position point, *i.e.*, ~~when~~ the first depression 16 formed in the sealing cap 12 ~~is has been~~ pushed over and aligned with the first bulge 15 formed on the connection element 5 so that the longitudinal carrier 11 inserted within the first channel 10 is prevented from escaping from the channel 10 formed in the connection element 5 but the longitudinal carrier 11

10 is free to longitudinally move with respect to the connection element 5 so that the bone and/or bone fragments attached to the bone fixation means 1 may be repositioned. After repositioning is completed, the sealing cap 12 is placed in the second or third latch position and locked. The tensioning means 13 is then tightened by means of the screwdriver so that ~~and~~ the longitudinal carrier 11 inserted in the first channel 10 is ~~blocked in the connection element 5. When the~~

15 tensioning means 13 is being tightened, the longitudinal carrier 11 is pressed onto the screw bone head 30 of the bone fixation means 1, which, in turn, clamps the head 30 in-between with the result that this is clamped between the shoulder 9 formed on the lower end 7 of the connection element 5 and the longitudinal carrier 11, thus fixing the position of ~~and~~ the bone fixation means 1 together with the longitudinal carrier 11 with respect to ~~is blocked in the connection element 5.~~

20 [0032] Fig. 5 illustrates an embodiment of the device according to the invention that differs from the embodiments described above only in that the screw head 30 of the bone fixation means 1 is secured against falling out of the cavity 8 by means of a securing means 35 ~~from driving out of the cavity 8. As shown, the~~ ~~The~~ securing means 35 comprises a pin 37 that is pressed, *for example*, in a hole 38 running transverse to the central axis 2 and which extends

25 into the cavity 8. The hole 38 is arranged axially between the rear end 41 of the screw bone head 30 of the bone fixation means 1 and the upper end 6 of the connection element 5. Alternatively, the connection element 5 may include ~~Instead of a hole 38, several holes 38 spread across the circumference of the connection element 5 for receiving width and~~ ~~several pins 37 can also be provided as securing means 35.~~

30 [0033] Fig. 6 shows an embodiment of the device according to the invention wherein the securing means 35 may be in the form of ~~is carried out by~~ a snap ring 39 instead of by one or several pins 37. The snap ring 39 is received within a groove 40 formed on ~~positioned at~~ the rear end 41 of the screw head 30 and which protrudes into the cavity 8 ~~so that the cavity 8 is tapered there towards its upper end 6~~. The groove 40 is arranged axially in such a way that the snap ring

39 inserted therein does not extend beyond ~~exceed~~ the rear end 41 of the screw head 30 towards the upper end 6 of the connection element 5, which means that the longitudinal carrier 11 does not lie on the snap ring 39. To achieve this, for example, the ~~The~~ screw head 30 is ~~for this~~ purpose ~~designed, for example, reduced with a reduced diameter portion~~ at its rear end 41. That 5 ~~is, the screw head 30~~ and is provided at this rear end 41 with an axial segment 42 which has a diameter smaller than the screw ~~bone~~ head 30 thus forming a ~~The~~ shoulder 43 ~~formed by this~~ ~~segment 42 with reduced diameter will then be brought in contact with~~ for receiving the securing ~~means~~ device 35 provided here in the form of a snap ring 39, so that the screw head 30 can be arrested against axial movements towards the upper end 6 of the connection element 5 by the 10 ~~snap ring 39 in the cavity 8. The reduced diameter portion segment 42 of the screw head 30~~ passes through the ring-shaped opening of the snap ring 39 and protrudes ~~at the end~~ beyond the snap ring 39, so that the longitudinal carrier 11 can rest on ~~at~~ the rear end 41 of the screw head 30. Therein, in use, the securing means 35 prevents the screw head 30 from axial movement towards the upper end 6 of the connection element 5.